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# Significance of multiple slip and nanoparticle shape on stagnation point flow of silver-blood nanofluid in the presence of induced magnetic field

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### ABSTRACT

Non-spherical nanoparticles have gained popularity for their ability in changing the thermophysical properties of a nanofluid. The current work focuses on studying the significance of multiple slip and nanoparticle shape on stagnation point flow of blood-based silver nanofluid considering chemical reaction, induced magnetic field, thermal radiation, and linear heat source which is beneficial in cancer therapy, biomedical imaging, hyperthermia, and tumor therapy. Relevant similarity transformations are effectuated in converting the mathematically modeled governing equations into a system of ODEs and are then numerically resolved in MATLAB employing the adaptive Runge-Kutta method and the Newton Raphson method. Observations on the consequence of differing parameters on varying attributes are achieved via tables and graphs. Additionally, the shape effect of nanoparticles on various attributes is also evaluated. Linear heat source and thermal radiation parameters exhibit a constructive effect whereas the thermal slip parameter exhibits a destructive effect on temperature. Further, it is observed that the blade-shaped nanoparticle exhibits the greatest heat transfer rate followed by platelet, cylinder, and spherical-shaped nanoparticles, respectively.

### 1. Introduction

Nanofluid, discovered by Choi and Eastman [1], was known for its unparalleled heat transfer and cooling abilities. Choi proposed nanofluid as a suspension of nanoparticles (1–100 nm in size) and observed that the conventional fluid and nanofluid exhibit distinct physical and chemical properties. According to Ying-Qing et al. [2] and Oke et al. [3], the inherent nature of nanoparticles is bound to affect the temperature distribution. Neethu et al. [4] investigated the significance of the nanoparticle volume fraction on the hydromagnetic flow between two vertical porous plates moving in opposite directions based on the single-phase nanofluid model proposed by Tiwari and Das [5]. They observed a decline in the nanoliquid temperature profile due to augmenting nanoparticle volume fraction. However, augmenting nanoparticle volume fraction tends to increase the nanoliquid temperature in an unsteady nanoliquid flow past an inclined plate (see Mackolil and Mahanthesh [6]). A few studies exploring nanofluid flow can be seen in [7–11].

Particles of silver between 1 and 100 nm, called silver nanoparticles, have been proved to be beneficial in the medical field with their antibacterial properties and also due to their applicability in the treatment of many diseases; namely cancer (see [12–14]). Abbasi et al. [15] examined the peristaltic transport of silver-water nanofluid in the presence of constant applied magnetic field considering Ohmic heating, velocity slip, thermal slip, and Hall effects. They observed that the addition of 5% silver nanoparticles reduced the velocity and temperature of the base fluid by 10% and 16%, respectively. The dominating nature of silver nanoliquid over copper nanoliquid on the heat transfer rate was observed by Hayat et al. [16] and Sravanthi [17]. In addition, Hayat et al. [18] noted that the Bejan number is more for Ag-water nanofluid. The increment of the average Nusselt number by increasing the volume fraction of nanoparticles for typical nanofluid is more sensible than hybrid nanofluid in an enclosure with rotating heat sources (see Jamiatia [19]). The study on the hydrothermal and irreversibility behaviour of a biologically synthesized silver-water nanoliquid in a wavy microchannel heat sink, conducted by Al-Rashed et al. [20], revealed that the nanoliquid has a better cooling performance in comparison with pure water.

The nanoparticles can be categorized into spherical and non-spherical nanoparticles based on their physical shape. Different shaped nanoparticle exhibits different properties and different heat transfer capabilities (see Truong et al. [21]). Timofeeva et al. [22] analyzed the thermophysical properties of alumina nanofluid with different nanoparticle shapes; namely platelet, blade, brick, and cylinder; both practically and theoretically. Ellahi et al. [23] pointed out that the lowest

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| Nomenclature      |  | R <sub>d</sub><br>Sh <sub>x</sub> | Thermal radiation parameter<br>Local Sherwood number |
|-------------------|--|-----------------------------------|--|
| а, с              | Dimensional constants                          | Nu <sub>x</sub>                   | Local Nusselt number                                 |
| $D_B$             | Mass diffusivity $(m^2 s^{-1})$                | $Re_x$                            | Local Reynolds number                                |
| k <sub>r</sub>    | Reaction rate constant( $s^{-1}$ )             | <i>x</i> , <i>y</i>               | Cartesian coordinates(m)                             |
| $C_{slip}$        | Solutal slip parameter                         | $C_{\infty}$                      | ambient nanoparticle concentration                   |
| C                 | Fluid concentration                            | Le                                | Lewis number   |
| Т                 | Fluid temperature (K)                          |                                   |  |
| $C_W$             | Nanoparticle concentration near the wall       | Greek sy                          | mbols  |
| $T_W$             | Wall fluid temperature                         | θ                                 | Kinematic viscosity $(m^2 s^{-1})$                   |
| Cfr               | Local drag coefficient                         | η                                 | Dimensionless variable                               |
| a <sub>T</sub>    | Heat source coefficient                        | σ*                                | Stefan- Boltzmann constant                           |
| Pr                | Prandtl number                                 | λ                                 | Reciprocal of magnetic Prandtl number                |
| а                 | Radiative heat flux                            | $\alpha_m$                        | Magnetic diffusivity $(m^2s^{-1})$                   |
| 4r<br>Kr          | Chemical reaction parameter                    | φ                                 | Nanoparticle volume fraction                         |
| N <sub>1</sub>    | Temperature slip factor                        | ρ                                 | Density of the fluid $(kgm^{-3})$                    |
| C                 | Specific heat                                  | κ                                 | Thermal conductivity $(Wm^{-1}K^{-1})$               |
| $O_p$             | Velocity components $(ms^{-1})$                | $\mu_e$                           | Magnetic permeability ( $kgms^{-2}A^{-2}$ )          |
| и, <i>v</i><br>М. | Uniform magnetic field at infinity $(4m^{-1})$ | σ                                 | Electrical conductivity $(kg^{-1}m^{-3}s^{3}A^{2})$  |
| т                 | Ambient fluid temperature                      | β                                 | Magnetic parameter                                   |
|                   | Thermal din nerometer                          | α                                 | Thermal diffusivity $(m^2 s^{-1})$                   |
| I slip<br>1.☆     | Maan abaawtian aa Giaint                       |                                   |  |
| κ^                | Mean absorption coefficient                    | Subscript                         | s  |
| $Q_T$             | Linear heat source                             | nf                                | Nanofluid  |
| $N_2$             | Concentration slip factor                      | f                                 | Conventional fluid                                   |
| $M_e$             | Magnetic field at free stream                  |                                   |  |

velocity and highest temperature of the nanoliquid were caused by the sphere and disc-shaped particles, respectively for the mixed convective nanoliquid flow past a vertical lengthening permeable sheet. In addition, Benkhedda et al. [24] reported that the maximum friction factor is exhibited by the platelet-shaped silver-titanium dioxide nanoparticles. The reduction in the temperature profile of Cu - CuO/blood with the increasing shape factor values was revealed by Tripathi et al. [25]. A comparative analysis of  $Ti - H_2$ Oand $Ag - H_2$ Onanofluids on the effect of nanoparticle shape in a microchannel, conducted by Sindhu and Gireesha [26], showcased that the silver nanofluid exhibited higher entropy than the titanium nanofluid. They also observed that the entropy generation is high in the case of disc-shaped nanoparticles, followed by needle and sphere-shaped nanoparticles. Recently, Elnaqeeb et al. [27] investigated the dynamics of water conveying nanoparticles with various densities and shapes through a rectangular closed domain and observed that the heat transfer is maximal in the case of ternary-hybrid nanofluid made up of copper oxide, copper, and silver nanoparticles.

Blood is a connective tissue in fluid form (see Sembulingam and Sembulingam [28]). Blood flow utilizing nanoparticles are important in the medical industry for cancer treatment and drug delivery. The significance of partial slip and buoyancy on the blood-gold Carreau nanofluid flow over an upper horizontal surface of a paraboloid of revolution was investigated by Koriko et al. [29]. They observed that the maximum values for surface drag and the heat transfer rate was showcased by smaller values of Deborah number. The augmentation in the volume fraction of carbon nanotubes increased the blood temperature (see Khalid et al. [30]). Dinarvand et al. [31] pointed out that the use of CuOandCu hybrid nanoparticles reduced the haemodynamic effect of the capillary relative to the pure blood case. In addition, Khan et al. [32] numerically simulated the nonlinear radiative flow of Casson gold-nanoliquid through a stretched rotating rigid disk subject to Lorentz force utilizing the three-stage Lobatto method. Recently, Ashraf et al. [33] utilized the generalized differential quadrature method to explore the peristaltic flow of blood-based Casson nanomaterial containing platelet-shaped magnetite nanoparticles. Further, the significance of partial slip due to lateral velocity and viscous dissipation for blood-gold Carreau nanomaterial and dusty fluid was elucidated by

Koriko et al. [34]. A significant difference in the effect of partial slip on the dynamics of dusty fluid and blood-gold nanomaterial was observed.

Induced magnetic field (IMF) is the additional magnetic field that gets induced on electrically conducting fluid in the presence of an external magnetic field. This phenomenon is due to the impact of a larger magnetic Reynolds number. IMF has applications in MRI, glass manufacturing, geophysics, and MHD generators, etc. IMF paired with blood flow plays a decisive role in blood pumps, treatment of cardiac diseases and has many other biomedical applications. Kumari et al. [35] explored the flow and heat transfer of an electrically conducting fluid (which is at rest) over an elongating sheet in the presence of sources/sinks and induced magnetic field. Later, the MHD flow over a lengthening sheet in the presence of an induced magnetic field was reinvestigated by Ali et al. [36]. Iqbal et al. [37] scrutinized the influence of induced magnetic field on ferrofluid past a vertical stretching surface and observed that velocity profile enhanced for assisting flow with magnetic parameter. Gireesha et al. [38] numerically analyzed nanofluid stagnation point flow past a stretching surface attending IMF and found out that the induced magnetic field enhances with the intensifying hydromagnetic field. Iqbal et al. [39] elucidated the influence of induced magnetic fields on water-based copper and titanium dioxide nanofluids utilizing the Keller box method. An opposite relation was found to exist between magnetic parameter and temperature profile. Further, Amjad et al. [40] studied the influence of Lorentz force and induced magnetic field on Casson micropolar nanoliquid over a permeable curved stretching/shrinking surface.

Regarding stagnation point flow, the velocity of the fluid at the striking point of the rigid body is zero. It proposes many applications in engineering, industry, and physiological fluid flows. Ali et al. [41] extended the work of Mahapatra and Gupta [42] to analyze the hydromagnetic stagnation point flow of an electrically conducting fluid over a lengthening sheet in the presence of an induced magnetic field. Later, Junoh et al. [43] extended the work of Ali et al. [41] by considering the stagnation point flow past a stretching/shrinking sheet in a hybrid nanomaterial. Abbas et al. [44] explored the stagnation-point hybrid nanofluid flow over a slip surface. They adopted the Runge-Kutta-Fehlberg method to numerically solve the nonlinear system of differential equations and



Fig. 1. Figurative representation.

Α

| Table 1     |                  |                      |                     |            |     |           |
|-------------|------------------|----------------------|---------------------|------------|-----|-----------|
| Comparison  | of drag          | coefficient ( $Cf_x$ | $Re_x^{1/2}$ ) with | [47,62,63] | for | different |
| values when | $\phi = \beta =$ | 0.                   |                     |            |     |           |

| Α   | $Cf_x Re_x^{1/2}$ |                   |                   |               |  |
|-----|-------------------|-------------------|-------------------|---------------|--|
|     | Iqbal et al. [47] | Hayat et al. [62] | Hayat et al. [63] | Present study |  |
| 0.1 | -0.969386         | -0.96939          | -0.96937          | -0.9693861    |  |
| 0.2 | -0.918107         | -0.91811          | -0.91813          | -0.9181071    |  |
| 0.5 | -0.667263         | -0.66726          | -0.66723          | -0.6672637    |  |
| 0.7 | -0.433475         | -0.43346          | -0.43345          | -0.4334756    |  |
| 0.8 | -0.299388         | -0.29929          | -0.29921          | -0.2993888    |  |
| 0.9 | -0.154716         | -0.15458          | -0.1545471        | -0.1547167    |  |
| 1   | 0                 | 0                 | 0                 | 0             |  |



**Fig. 2.**  $f(\eta)$  for differing **A** values.

noted that the velocity is inversely proportional to the velocity ratio parameter. Al-Amri and Muthtamilselvan [45] investigated stagnation point nanofluid flow containing micro-organisms and found an enhanced



**Fig. 3.**  $f(\eta)$  for differing  $\beta$  values.

velocity profile due to augmenting stagnation parameter. Some other studies concerning stagnation point flow can be seen in [46–49].

The slip boundary condition characterizes the relative movement of fluid with the boundary. Multiple slip corresponds to the case when more than one slip (velocity, thermal, or solutal) condition is considered. Daniel et al. [50] reported that the augmenting velocity slip parameter slows the velocity profile. Khan et al. [51] and Amanulla et al. [52] noted that multiple slip effects have a positive impact on boundary layer flow. The decrease in the heat transfer rate due to the velocity slip parameter was observed by Ibrahim and Negera [53]. Further, a decrease in the temperature and concentration profile was noted due to the increased thermal and solutal slip parameter values, respectively (see Barik et al. [54]). A few studies discussing the slip effects can be seen in [55–58].

Motivated by the above-mentioned studies, it is noted that the effect of multiple slip, spherical and non-spherical (cylinder, platelet, and blade) nanoparticles on the stagnation point flow of silver-blood



**Fig. 4.**  $f(\eta)$  for differing  $\phi$  values.



**Fig. 5.**  $f'(\eta)$  for differing nanoparticle shapes.



**Fig. 6.**  $Cf_x Re_x^{1/2}$  for differing nanoparticle shapes and  $\beta$  values.



**Fig. 7.**  $Cf_x Re_x^{1/2}$  for differing nanoparticle shapes and  $\phi$  values.



**Fig. 8.**  $g'(\eta)$  for differing **A** values.

nanofluid in the presence of an induced magnetic field has not yet been studied. This paper attempts to fill this gap. In addition, linear heat source, chemical reaction and thermal radiation effects are incorporated. Further, thermal and solutal slip effects are also considered for a realistic approach. The present study has applications in cancer therapy, biomedical imaging, hyperthermia, and tumor therapy (see [21, 59–61]). The impact of pertinent parameters on the flow profiles has been analyzed with an emphasis on the following research questions:

- What is the significance of thermal slip and solutal slip parameters on the nanofluid temperature and nanofluid concentration, respectively?
- How does the nanoparticle shape affect the flow profiles?
- What is the variation in the nanofluid temperature with linear heat source, thermal radiation, and volume fraction of silver nanoparticles?
- How sensitive are the physical quantities with spherical and non-spherical nanoparticles?

# 2. Problem statement

Two-dimensional steady stagnation point flow over a linearly elongating sheet (Fig. 1) is considered under the ensuing assumptions:



**Fig. 9.**  $g'(\eta)$  for differing  $\beta$  values.



**Fig. 10.**  $g'(\eta)$  for differing  $\lambda$  values.

- (i) The expanding sheet is positioned along *xaxis* and blood-based silver nanofluid occupies the regiony > 0.
- (ii)  $U_w(x) = cx$  and  $U_e(x) = ax$  corresponds to the velocity of the lengthening sheet and the free stream, respectively.
- (iii) Induced magnetic field vector,  $M = (M_1, M_2)$  is considered with  $M_1 \& M_2$  being the magnetic integrants along *x* and *y* direction, respectively.
- (iv) Chemical reaction, linear heat source, thermal radiation, and nanoparticle shape (sphere, cylinder, platelet, and blade) effects are incorporated.
- (v) Thermal and solutal slip effects are also considered.

Governing equations [46–48,54] takes the form:

$$\frac{\partial u}{\partial x} + \frac{\partial v}{\partial y} = 0 \tag{1}$$

$$\frac{\partial M_1}{\partial x} + \frac{\partial M_2}{\partial y} = 0 \tag{2}$$



**Fig. 11.**  $g'(\eta)$  for differing nanoparticle shapes.



**Fig. 12.**  $\theta(\eta)$  for differing **A** values.

$$u\frac{\partial u}{\partial x} + v\frac{\partial u}{\partial y} - \frac{\mu_e}{4\pi\rho_{nf}} \left( M_1 \frac{\partial M_1}{\partial x} + M_2 \frac{\partial M_1}{\partial y} \right)$$
$$= U_e \frac{dU_e}{dx} - \frac{\mu_e M_e}{4\pi\rho_{nf}} \frac{dM_e}{dx} + \left(\frac{\mu_{nf}}{\rho_{nf}}\right) \frac{\partial^2 u}{\partial y^2}$$
(3)

$$u\frac{\partial M_1}{\partial x} + v\frac{\partial M_1}{\partial y} - M_1\frac{\partial u}{\partial x} - M_2\frac{\partial u}{\partial y} = \alpha_m\frac{\partial^2 M_1}{\partial y^2}$$
(4)

$$u\frac{\partial T}{\partial x} + v\frac{\partial T}{\partial y} = \alpha_{nf}\frac{\partial^2 T}{\partial y^2} + \frac{q_T}{\left(\rho C_p\right)_{nf}}\left(T - T_\infty\right) - \frac{1}{\left(\rho C_p\right)_{nf}}\frac{\partial q_r}{\partial y}$$
(5)

$$u\frac{\partial C}{\partial x} + v\frac{\partial C}{\partial y} = D_B \frac{\partial^2 C}{\partial y^2} - k_r (C - C_\infty)$$
(6)



**Fig. 13.**  $\theta(\eta)$  for differing  $\phi$  values.



**Fig. 14.**  $\theta(\eta)$  for differing  $Q_T$  values.

with

$$u = U_w(x) = cx, \ v = 0, \ \frac{\partial M_1}{\partial y} = M_2 = 0, \ T = T_w + N_1 \frac{\partial T}{\partial y}, \ C$$
$$= C_w + N_2 \frac{\partial C}{\partial y}; \ at \ y = 0$$

$$u \to U_e(x) = ax, M_1 \to M_e(x) = M_0 x, \ T \to T_\infty, \ C \to C_\infty; as \ y \to \infty$$

where  $\alpha_m = \frac{1}{4\pi\mu_e\sigma_{nf}}$  represents the magnetic diffusivity.

Introducing the following similarity transformations:

$$\begin{split} u &= cxf'(\eta), \ v = -\sqrt{c\partial_f}f(\eta), \ M_1 = M_0xg'(\eta), \ M_2 = -M_0\sqrt{\frac{\partial_f}{c}}g(\eta), \\ \eta &= y\sqrt{\frac{c}{\partial_f}}, \ \theta(\eta) = \frac{T - T_\infty}{T_w - T_\infty}, \ \psi(\eta) = \frac{C - C_\infty}{C_w - C_\infty} \ . \end{split}$$

and applying linearized Roseland approximation in equations (1) - (6), we get:



**Fig. 15.**  $\theta(\eta)$  for differing  $R_d$  values.



**Fig. 16.**  $\theta(\eta)$  for differing  $T_{slip}$  values.

$$f'' = A_1 A_2 \left\{ (f')^2 - f f'' - A^2 - \frac{\beta}{A_2} \left\{ (g')^2 - g g'' - 1 \right\} \right\}$$
(7)

$$g'' = \frac{A_5}{\lambda} \{ g f'' - f g'' \}$$
(8)

$$\theta'' = \frac{-Pr\{A_3 f \theta' + Q_T \theta\}}{A_4 + \frac{4}{3}R_d}$$
(9)

$$\psi'' = Kr \ Le \ \psi - Le \ f \ \psi' \tag{10}$$

subject to the boundary conditions

$$\begin{split} f(0) &= 0, f^{'}(0) = 1, \ g(0) = 0, \ g^{\prime\prime}(0) = 0, \ \theta(0) = 1 + T_{slip} \ \theta^{'}(0), \ \psi(0) \\ &= 1 + C_{slip} \ \psi^{'}(0). \end{split}$$

$$f'(\infty) \rightarrow A, g'(\infty) \rightarrow 1, \theta(\infty) \rightarrow 0, \psi(\infty) \rightarrow 0$$

where the dimensionless parameters are :



**Fig. 17.**  $\theta(\eta)$  for differing nanoparticle shapes.



| Property | Blood (base fluid) | Silver (nanoparticle) |
|----------|--------------------|-----------------------|
| ρ        | 1063               | 10490                 |
| $C_p$    | 3594               | 235                   |
| ĸ        | 0.492              | 429                   |
| σ        | 0.8                | $63 * 10^7$           |



**Fig. 18.**  $Nu_x Re_x^{-1/2}$  for differing nanoparticle shapes and  $\phi$  values.

$$A = \frac{a}{c}, \ \beta = \frac{\mu_e}{4 \pi \rho_f} \left(\frac{M_0}{c}\right)^2, \ \lambda = \frac{1}{4 \pi \mu_e \sigma_f \theta_f}, \ Pr = \frac{(\mu C_p)_f}{\kappa_f}, \ R_d = \frac{4 \sigma^* T_\infty^3}{k^* \kappa_f},$$
$$Q_T = \frac{q_T}{c (\rho C_p)_f}, \ Kr = \frac{k_r}{c}, \ Le = \frac{\theta_f}{D_B}, \ T_{slip} = N_1 \ \sqrt{\frac{c}{\theta_f}}, \ C_{slip} = N_2 \ \sqrt{\frac{c}{\theta_f}}.$$

The nanofluid models [24] incorporated are :

| Spherical  | Non-spherical   |
|--|---|
| $rac{\mu_{nf}}{\mu_f} = rac{1}{\left(1-\phi ight)^{2.5}} = rac{1}{A_1}$ | $rac{\mu_{nf}}{\mu_f} = 1 + A_{shape} \; \phi + B_{shape} \; \phi^2 \; = rac{1}{A_1}$ |
|  | (continued on next column)  |



**Fig. 19.**  $Nu_x Re_x^{-1/2}$  for differing nanoparticle shapes and  $Q_T$  values.



**Fig. 20.**  $Nu_x Re_x^{-1/2}$  for differing nanoparticle shapes and  $R_d$  values.



Fig. 21.  $Nu_x Re_x^{-1/2}$  for differing nanoparticle shapes and  $T_{slip}$  values.



**Fig. 22.**  $\psi(\eta)$  for differing **A** values.





(continued)

| Spherical | Non-spherical   |
|-----------|---|
|           | $A_2 \;= rac{ ho_{nf}}{ ho_f} = (1\;-\phi) + \phiigg(rac{ ho_{Ag}}{ ho_f}igg)$  |
|           | $A_3 = rac{( ho C_p)_{\eta f}}{( ho C_p)_f} = (1-\phi) + \phiiggl(rac{( ho C_p)_{Ag}}{( ho C_p)_f}iggr)$  |
|           | $A_4 = \frac{\kappa_{nf}}{\kappa_f} = \frac{\kappa_{Ag} + (s-1)\kappa_f - (s-1)\phi(\kappa_f - \kappa_{Ag})}{\kappa_{Ag} + (s-1)\kappa_f + \phi(\kappa_f - \kappa_{Ag})}$   |
|           | $A_5=rac{\sigma_{nf}}{\sigma_f}=1+rac{3\Big(rac{\sigma_{Ag}}{\sigma_f}-1\Big)\phi}{\Big(rac{\sigma_{Ag}}{\sigma_f}+2\Big)-\Big(rac{\sigma_{Ag}}{\sigma_f}-1\Big)\phi}$ |

| The nanoparticle shape properties [24] are: |        |          |          |       |  |  |
|---|--------|----------|----------|-------|--|--|
|   | Sphere | Cylinder | Platelet | Blade |  |  |
| Ashape                                      | -      | 13.5     | 37.1     | 14.6  |  |  |
| Bshape                                      | -      | 904.4    | 612.6    | 123.3 |  |  |
| Shape factor,s                              | 3      | 4.9      | 5.7      | 8.6   |  |  |



**Fig. 24.**  $\psi(\eta)$  for differing *Kr* values.



**Fig. 25.**  $\psi(\eta)$  for differing  $C_{slip}$  values.

| Table 3                                    |                                      |                  |
|--|--------------------------------------|------------------|
| Variation in $Sh_x Re_x^{-1/2}$ when $A =$ | 0.5, $\beta = 0.1$ , $\lambda = 0.5$ | & $\phi = 0.1$ . |

| Kr  | Le  | $C_{slip}$ | $Sh_x Re_x^{-1/2}$ | 2        |          |        |
|-----|-----|------------|--------------------|----------|----------|--------|
|     |     |            | Sphere             | Cylinder | Platelet | Blade  |
| 1.5 | 0.3 | 0.3        | 0.6166             | 0.6263   | 0.6261   | 0.6217 |
| 2   |     |            | 0.6773             | 0.6852   | 0.6850   | 0.6815 |
| 2.5 |     |            | 0.7298             | 0.7363   | 0.7362   | 0.7333 |
| 2   | 0.2 | 0.3        | 0.5737             | 0.5808   | 0.5807   | 0.5774 |
|     | 0.3 |            | 0.6773             | 0.6852   | 0.6850   | 0.6815 |
|     | 0.4 |            | 0.7594             | 0.7675   | 0.7674   | 0.7638 |
| 2   | 0.3 | 0.2        | 0.7265             | 0.7355   | 0.7354   | 0.7313 |
|     |     | 0.3        | 0.6773             | 0.6852   | 0.6850   | 0.6815 |
|     |     | 0.4        | 0.6343             | 0.6412   | 0.6411   | 0.6380 |

Physical quantities [47,49] (in dimensionless form) are given by:

| Local drag coefficient : | $\mu_{nf} \frac{\partial u}{\partial u}\Big _{v=0}$   |
|--------------------------|---|
|                          | $Cf_{x} = \frac{\tau_{\omega}}{\rho_{f} (U_{W})^{2}} = \frac{-\eta}{\rho_{f} (U_{W})^{2}} \Rightarrow Cf_{x} Re_{x}^{1/2} = \frac{f'(0)}{A_{1}}.$                                       |
| Local Nusselt number :   | $x q_{\omega} = -x \left( \kappa_{nf} \frac{\partial T}{\partial y} - q_r \right)  _{y=0} \qquad (t - 4p) q_r (t)$  |
| Local Sherwood number :  | $Nu_{x} = \frac{1}{\kappa_{f} (T_{W} - T_{\infty})} = \frac{1}{\kappa_{f} (T_{W} - T_{\infty})} \Rightarrow Nu_{x} Re_{x}^{-1/2} = -\left(A_{4} + \frac{1}{3}R_{d}\right) \theta (0) .$ |
|                          | $Sh_x = \frac{x \ q_m}{D_n \ (C_w - C_w)} = \frac{-x \ D_B}{D_n \ (C_w - C_w)} \Rightarrow Sh_x \ Re_x^{-1/2} = -\psi'(0) \ .$  |

#### 3. Numerical scheme and validation

Equations(7) - (10) together with the boundary conditions are numerically resolved in MATLAB employing the adaptive Runge-Kutta method [64] (for solving) and Newton Raphson (for shooting). This is accomplished by initially assuming:

$$\begin{split} \Xi_{1} &= f, \ \Xi_{2} = f, \ \Xi_{3} = f'', \ \Xi_{3} = f'', \\ \Xi_{4} &= g, \ \Xi_{5} = g', \ \Xi_{6} = g'', \ \Xi_{6}' = g'', \\ \Xi_{7} &= \theta, \ \Xi_{8} = \theta', \ \Xi_{8}' = \theta'', \\ \Xi_{9} &= \psi, \ \Xi_{10} = \psi', \ \Xi_{10}' = \psi''. \\ \text{The reduced system of first-order OE} \end{split}$$

The reduced system of first-order ODE is given by:  

$$\Xi_{1}' = \Xi_{2},$$

$$\Xi_{2}' = \Xi_{3},$$

$$\Xi_{3}' = A_{1} A_{2} \left\{ (\Xi_{2})^{2} - \Xi_{1} \Xi_{3} - A^{2} - \frac{\beta}{A_{2}} \left\{ (\Xi_{5})^{2} - \Xi_{4} \Xi_{6} - 1 \right\} \right\},$$

$$\Xi_{4}' = \Xi_{5},$$

$$\Xi_{5}' = \Xi_{6},$$

$$\Xi_{6}' = \frac{A_{5}}{\lambda} \left\{ \Xi_{4} \Xi_{3} - \Xi_{1} \Xi_{6} \right\},$$

$$\Xi_{7}' = \Xi_{8},$$

$$\Xi_{8}' = \frac{-Pr \left\{ A_{3} \Xi_{1} \Xi_{8} + Q_{7} \Xi_{7} \right\}}{A_{4} + \frac{4}{3}R_{d}},$$

$$\Xi_{9}' = \Xi_{10},$$

$$\Xi_{10}' = Kr \ Le \ \Xi_9 - Le \ \Xi_1 \ \Xi_{10} \ .$$

with

$$\begin{split} \Xi_1(0) &= 0, \; \Xi_2(0) = 1, \; \Xi_3(0) = \Gamma_1, \; \Xi_4(0) = 0, \; \Xi_5(0) = \Gamma_2, \; \Xi_6(0) = 0, \\ \Xi_7(0) &= 1 + \mathit{T_{slip}} \; \Gamma_3, \; \Xi_8(0) = \Gamma_3, \; \Xi_9(0) = 1 + \mathit{C_{slip}} \; \Gamma_4, \; \Xi_{10}(0) = \Gamma_4 \; . \end{split}$$

where  $\Gamma_1$ ,  $\Gamma_2$ ,  $\Gamma_3$ ,  $\Gamma_4$  &  $\Gamma_5$  are estimated using the Newton Raphson method with a suitable initial guess.

Validity of the code for the current problem has been adjudged through a restrictive correspondence of the present work with prior published works [47,62,63] (see Table 1) and a commendable agreement is noted.

#### 4. Results and discussion

The consequence of influential parameters on velocity( $f'(\eta)$ ), concentration( $\psi(\eta)$ ), temperature( $\theta(\eta)$ ), induced magnetic field( $g'(\eta)$ ) profiles and physical quantities are illustrated via Figs. 2–25. Prandtl number(Pr) and infinity are fixed at 21 and 5, respectively. Thermophysical properties of base fluid (blood) and silver (nanoparticle) are showcased in Table 2.

Fig. 2 elucidates the positive impact of the stretching parameter (*A*) on  $f'(\eta)$  meaning that an augmentation in stretching parameter results in the escalation of  $f'(\eta)$ . Fig. 3 describes the deviations in  $f'(\eta)$  with  $\beta$  (magnetic parameter). An increase in  $\beta$  tends to increase  $f'(\eta)$ . Fig. 4 bespeaks the deviations in  $f'(\eta)$  with respect to  $\phi$  (nanoparticle volume fraction). It can be observed that  $f'(\eta)$  decreases for augmenting  $\phi$  values. This can be physically associated with the fact that ascending  $\phi$  values, as pointed out by Mackolil and Mahanthesh [6], increases the nanofluid viscosity which in turn decreases the nanofluid velocity. The nanoparticle shape effect on velocity profile is depicted in Fig. 5. The highest nanofluid velocity profile is exhibited by cylinder-shaped silver nanoparticles followed by platelet, blade, and spherical-shaped nanoparticles, respectively.

Figs. 6 & 7 elucidate the parallel effect of  $\beta \& \phi$  with the differing nanoparticle shapes on  $Cf_x Re_x^{1/2}$ . It is perceived that  $Cf_x Re_x^{1/2}$  is a decreasing function of  $\phi$  and an increasing function of  $\beta$ . Further, it can be observed that the drag coefficient is highest for spherical-shaped silver nanoparticles and least for cylindrically shaped silver nanoparticles.

Fig. 8 displays the negative impact of A on  $g'(\eta)$  whereas Fig. 9 displays the positive impact of  $\beta$  ong'( $\eta$ ). A commendable agreement is noted between the results observed in Figs. 8 & 9 and the work of Ali et al. [41]. Fig. 10 explains the mixed effect of  $\lambda$  (reciprocal of magnetic Prandtl number) ong'( $\eta$ ). Initially, elevating  $\lambda$  values decays  $g'(\eta)$  and afterwards, a reversed trend is observed. Fig. 11 represents nanoparticle shape effect ong'( $\eta$ ). The highest and lowest induced magnetic field profiles are recorded by cylindrical and spherical shaped silver nanoparticles, respectively.

The consequence of A on  $\theta(n)$  is graphed in Fig. 12. A decline in temperature is noted for the increasing A values. Fig. 13 throws light into the constructive nature of  $\phi$  on $\theta(\eta)$ . Physically, the improvement in  $\theta(\eta)$  is due to the increased thermal conductivity of fluid caused by the hike in nanoparticle volume fraction (see Mackolil and Mahanthesh [65]). In addition, the inherent nature of nanoparticles is bound to affect the temperature distribution (see Ying-Qing et al. [2] and Oke et al. [3]). The influence of  $Q_T$  (linear heat source parameter) and  $R_d$  (thermal radiation parameter) on  $\theta(\eta)$  is analyzed in Figs. 14 & 15, respectively. Both parameters tend to increase  $\theta(\eta)$ . This can be associated with the fact that an increase in  $Q_T \& R_d$  as mentioned by Mackolil and Mahanthesh [66] supplies supplemental energy to the system which triggers a surge  $in\theta(\eta)$ . Biologically, the increase in temperature profiles due to augmenting nanoparticle volume fraction, linear heat source, and thermal radiation unveils that the nanofluid can be used for killing tumors or cancerous cells (see Jama et al. [67]). The effect of  $T_{slip}$  (thermal slip parameter) is analyzed with the aid of Fig. 16. It is noted that augmenting  $T_{slip}$  values lead to a decrease in $\theta(\eta)$ . Augmentation in the thermal slip parameter as pointed out by Sabu et al. [58] reduces the sensitivity of the fluid flow within the boundary layer, which reduces the amount of heat produced and thereby reduces the temperature. The impact of nanoparticle shape on  $\theta(\eta)$  is explained in Fig. 17. The blade-shaped silver nanoparticles contribute the most towards  $\theta(\eta)$  and cylinder-shaped silver nanoparticles contribute the least towards $\theta(\eta)$ .

The parallel effect of  $\phi$ ,  $Q_T$ ,  $R_d \& T_{slip}$  with the differing nanoparticle shapes on  $Nu_x Re_x^{-1/2}$  is elucidated in Figs. 18–21. It is seen that  $\phi \& R_d$  promotes  $Nu_x Re_x^{-1/2}$  whereas  $Q_T \& T_{slip}$  demotes  $Nu_x Re_x^{-1/2}$ . A significant rise in the heat transfer rate is showcased by the blade-shaped silver nanoparticles followed by platelet, cylinder, and spherical-shaped nanoparticles, respectively.

Variation in  $\psi(\eta)$  for differing *A* values is demonstrated in Fig. 22 and it is perceived that *A* has a negative effect on $\psi(\eta)$ . Fig. 23 elucidates the effect of *Le* (Lewis number) on $\psi(\eta)$ .  $\psi(\eta)$  decreases with augmenting *Le* values. Fig. 24 explains the negative impact of *Kr* (chemical reaction parameter) on  $\psi(\eta)$ . This can be associated with the fact that augmenting *Kr* values as pointed out by Neethu et al. [4] eats up the nanoparticle which decreases  $\psi(\eta)$ . Biologically, consumption of more nanoparticles is directly proportional to improved medication and hyperthermia (see Kaur et al. [68]). The impact of  $C_{slip}$  (solutal slip parameter) on  $\psi(\eta)$  is graphed in Fig. 25. It is seen that increasing  $C_{slip}$ values help in decreasing $\psi(\eta)$ . The consequence of pertinent parameters on  $Sh_x Re_x^{-1/2}$  is explained in Table 3. It is perceived that Kr & Lehave a positive impact on  $Sh_x Re_x^{-1/2}$  and  $C_{slip}$  hurts  $Sh_x Re_x^{-1/2}$ . In addition, it is observed that the cylinder-shaped silver nanoparticles offer the highest  $Sh_x Re_x^{-1/2}$  value.

## 5. Conclusion

The influence of thermal and solutal slip on the stagnation point flow of blood-based silver nanomaterial in the presence of an induced magnetic field has been examined. The significance of spherical and nonspherical silver nanoparticles on the flow profiles and physical quantities has been analyzed. The key points drawn from the study are:

- Nanofluid temperature and nanofluid concentration reduce with increasing values of thermal slip and concentration slip parameters, respectively.
- Velocity and induced magnetic field profiles are least affected by spherical-shaped silver nanoparticles and highly affected by cylinder-shaped silver nanoparticles. Blade shaped silver nanoparticles contribute the most whereas cylinder-shaped silver nanoparticles contribute the least towards the nanofluid temperature.
- Nanofluid temperature ascends with augmenting linear heat source, thermal radiation parameter, and volume fraction of silver nanoparticles.
- Blade shaped silver nanoparticles offer an increased heat transfer rate over the other nanoparticle shapes and cylinder-shaped silver nanoparticles exhibit the highest mass transfer rate. A significant rise in the surface drag is brought out by the spherical-shaped silver nanoparticles followed by blade, platelet, and cylinder-shaped nanoparticles.

### CRediT authorship contribution statement

Alphonsa Mathew: Conceptualization, Data curation, Formal analysis, Methodology, Writing – original draft, Writing – review & editing. Sujesh Areekara: Conceptualization, Data curation, Formal analysis, Methodology, Writing – original draft, Writing – review & editing. A.S. Sabu: Conceptualization, Data curation, Formal analysis, Methodology, Writing – original draft, Writing – review & editing. S. Saleem: Writing – review & editing.

# **Declaration of Competing Interest**

This is to certify that we the authors of the paper entitled 'Significance of multiple slip and nanoparticle shape on stagnation point flow of silver-blood nanofluid in the presence of induced magnetic field' have no conflicts of interest.

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